Variable-focal lens using electroactive polymer actuator

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abstract

We present a simple and cost-effective design and fabrication process of a liquid-filled variable-focal lens using electroactive polymer as an actuator. The lens is made of soft polymer material, its shape and curvature can be controlled by pneumatic pressure. As an actuator, we used a carbon-polymer composite (CPC); likewise it is possible to use any other ionic EAP. The device is composed of elastic membrane upon a circular lens chamber, a reservoir of liquid, and a channel between them. It is made of three layers of polydimethylsiloxane (PDMS), bonded using the technics of partial curing. The channels and reservoir are filled with incompressible liquid after curing process. A CPC actuator is mechanically attached to reservoir to compress or decompress the liquid. Squeezing the liquid between the reservoir and the lens chamber will push the membrane inward or outward resulting in the change of the shape of the lens and alteration of its focal length. Depending on the pressure the lens can be plano-convex or plano-concave or even switch between the two configurations. With only a few minor modifications it is possible to fabricate bi-convex and bi-concave lenses. We report on a 1 mm diameter lens that can be converging or diverging with the focal length from infinity to 17 mm. The 5x15mm CPC actuator with the working voltage of only up to ±2.5V was capable to alter within the full range of the focal length in 10 seconds.

**Keywords:** Liquid lens, variable-focal, electroactive polymer, PDMS, CPC actuator

1. Introduction

Variable-focal lenses have been researched for years. There are several fields including beam steering and portable imaging where usage of tunable lenses could give an extra value. Variable-focal length lenses could be constructed without using mechanical translational movement thus noiseless design of the lens system is possible.

Tunable lenses could be classified as follows: electrowetting, gel type, and liquid lenses. Electrowetting lens is based on a drop of liquid which shape is changed by applied voltage. Alteration of optical power is obtained by electrowetting behavior of the droplet and the changes of its contact angle. Although these lenses have fast response time, authors have found it hard to reach larger apertures {{1040 Jong-Moon Choi 2008}}. Moreover, relatively high voltage (~50V) is required to operate {{1056 Hendriks,B.H.W. 2005}}{{1007 Shimizu,I. 2009}}.

Gel type lens is composed of elastic material that is contracted and expanded thus changing the radius of curvature. For instance SMA actuator has been used to control contraction/expansion {{1040 Jong-Moon Choi 2008}}. Gel type lenses are relatively resistant to vibrations and shocks but have limited focal range.

Finally, the concept of liquid lens uses three key elements: transparent elastic membrane (often made of polydimethylsiloxane – PDMS), liquid, and an actuator. The membrane is deformed as a result of pneumatic pressure in the liquid. As a result of deforming the membrane, the radius of curvature of the lens is changed and optical power is altered. For pressure control, different actuators like an external pump {{1024 Lin,Wei-Cheng 2008}} or directly connected piezostack actuator {{1021 Oku,H. 2009}} have been used. Compared to electrowetting lens, liquid lenses are able to produce wider range of focal length and the design of the lens is rather simple. Considering liquid lenses, there is also an option to choose between different actuators allowing the system to be more dynamic.

Electroactive polymers (EAPs) are materials that change their shape and size in response to applied voltage. These materials have large potential in the fields of microfluidics, robotics, and biomedicine. Although ionic EAPs, like ionic polymer metal composites (IPMCs), have been developed for years, they have been rather rarely used to drive tunable lenses. However, Shimizu *et al* {{1007 Shimizu,I. 2009}} have demonstrated a promising variable-focal liquid lens system which has four IPMC strips attached to deformable lens membrane. By moving the edges of a membrane towards the liquid, the deformation occurs in the opposite direction. Therefore, a variable-focal length is achieved. IT WOULD BE NICE TO FIND SOME SERIOUS CAP IN THIS DEVICE☺. Synchronization of all the 4 IPMC strips?

Recently there has been an increasing interest in ionic EAPs based on carbon. These EAPs are called carbon-polymer composites (CPCs). CPC is a three layer actuator which electrodes are made of porous carbon material, base polymer, and ionic liquid. Unlike IPMC, the relaxation of CPC actuator is notably slower due to the low speed of desorption of ions of the ionic liquid from the porous carbon. Another advantage of CPC is. Further details about the CPC actuator used in this paper are described in {{1016 Torop,Janno 2009}}. {{1058 Torop,Janno 2009; 1057 Torop,Janno 2010}}

In current paper we propose a novel approach to construct liquid-filled variable-focal lens by using partial curing technique of PDMS and CPC actuator. In this configuration large focal range is obtained by using the voltage in the range of only 2.5 volts.

2. STRUCTURE OF THE LENS

Mingi seletav joonis, aga mitte see solidworks, lihtsamat on vaja

### Aktuaatori poolt avaldatav rõhk

To test the pressure range where CPC actuator is operating, simple experiment was carried out. Little rubber balloon was attached to pressure sensor (Smartec SPD002GAsil) and squeezed by CPC actuator with an actuating voltage of 2.5V. Voltage was set back to zero at the time t=100. Fig. 2.1 shows results where actuator position is varied throughout the measurements. According to the results, the maximum pressure ~1 kPa was reached during the measurements.



### Matemaatika

The center deformation of the lens membrane can be expressed by following equation (REF to roarks stress &strain):

|  |  |  |
| --- | --- | --- |
|  | $$y\_{c}=\frac{-pr^{4}}{64D}$$ | (1) |

where $y\_{c}$ is the center deformation, p is the pressure applied to the membrane, r is the radius of the lens, and D is the plate constant that is obtained from:

|  |  |  |
| --- | --- | --- |
|  | $$D=\frac{Et^{3}}{12(1-ν^{2})}$$ | (2) |

where $E$ is the modulus of elasticity of the PDMS, $t$ is the thickness of the lens membrane, and $ν$ is the Poisson’s ratio of the PDMS.

Moreover, if center deformation is known we can find focal length by assuming the lens membrane profile to be sphere:

|  |  |  |
| --- | --- | --- |
|  | $$R=\frac{r^{2}}{2y\_{c}}+\frac{y\_{c}}{2}$$ | (3) |

where $R$ is the radius of curvature, $r$ is the radius of the membrane, and $y\_{c}$ is the center deformation of the membrane. Now focal length could be found by following equation:

|  |  |  |
| --- | --- | --- |
|  | $$f=\frac{R}{n-1}$$ | (4) |

Where $f$ is the focal length, $R$ is the radius of curvature of the lens, and $n$ is the refractive index of the PDMS.

### Comsoli arvutused

Joonised 5.3 ja 5.4

Equations X

Equations X

Fig. 2.2 Focal length depending on thickness.

3. Fabrication

Ainult prototüüp 3. Natuke bondimisest ja vormist ja lõplikust kujust.

To achieve lens system with a structure as described in Sec. 2, special mold for the middle layer is needed (Fig 3.1). We used CNC milling machine (Wabeco, F1410LF) and Teflon to construct the mold. Also simple rectangular mold was created for bottom layer.

PDMS (Sylgard 184) was obtained from Dow Corning. Curing agent and base polymer was mixed using the ratio 1:10. Next, mixture was carefully stirred for about 5 minutes after which it was degased in vacuum oven at room temperature for another 10 minutes. Then, PDMS was casted into the molds and the film was fabricated using a universal casting applicator (MODEL HERE). All three layers were heated at 60-65 C° for 20 minutes. By this proccess, enough crosslinks are formed in PDMS to remove middle layer from the mold without damage, still leaving the ability to bond to another PDMS layer by further curing. Next, the removed layer was attached between other layers and heated at 90 C° for about an hour to final cure the PDMS. Finally the liquid was injected into the lens system via syringe. Ethylene glycol was used as the liquid, because of its very similar refraction index to PDMS (~1.43) (REF). This enables us not to consider the light fraction between liquid and PDMS. Because of the toxicity of ethylene glycol, the usage of this device is limited in the fields of biomedicine. Instead ethylene glycol, water has been used (REF), but in that case vaporization of the water through PDMS has to be considered. For example water vaporization has been avoided using PDMS surface treatment with oxygen plasma (REF). The result of ethylene glycol filled tunable lens is shown in Fig 3.2.

Fig. 3.2

4. Experimental

Pilt 6.8 

Vedeliku valik



Pilt 7.1 ja seletus

Pilt 8.1 ja seletus

5. Conclusions

We have demonstrated a simple and cheap solution to construct a variable focal lens using carbon-polymer composite actuator, CNC milling machine and partial PDMS curing technology. According to measurements the focal length from ∞ to 17 mm was achieved. The result is limited to 40 mm because of the measurement technique that requires a high resolution CCD and a high quality screen for larger focal length values.

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