Journal of Intelligent Material Systems & Structures

A Distributed Model of Ionomeric Polymer Metal Composite

Journal:			
Manuscript ID:			
Manuscript Types:	Original Article		
Date Submitted by the Author:	n/a		
Complete List of Authors:	Punning, Andres; Tartu University Institute of Technology, IMS Lab Johanson, Urmas; Tartu University Institute of Technology, IMS Lab Anton, Mart; Tartu University Institute of Technology, IMS Lab Aabloo, Alvo; Tartu University Institute of Technology, IMS Lab Kruusmaa, Maarja; Tartu University Institute of Technology, IMS Lab		
Keyword:	Electroactive polymers, Actuator, IPMC, Distributed RC lines		
Abstract:	This paper presents a novel model of an IPMC (Ionomeric polymer metal composite). An IPMC is modeled as a lossy RC distributed line. Unlike other electromechanical models of an IPMC, the distributed nature of our model permits modelling the non-uniform bending of the material. Instead of modeling the tip deflection or uniform deformation of the material, we model the changing curvature. The transient behavior of the electrical signals as well as the transient bending of IPMC are described by Partial Differential Equations. Implementing the proper initial and boundary conditions results with the analytical description of the possibly nonuniform transient behavior of IPMC.		



A Distributed Model of Ionomeric Polymer Metal Composite

A. Punning*, U. Johanson, M. Anton, A.Aabloo, M.Kruusmaa Institute of Technology, Tartu University, Nooruse 1, Tartu 50411, Estonia

ABSTRACT: This paper presents a novel model of an IPMC (Ionomeric polymer metal composite). An IPMC is modeled as a lossy RC distributed line. Unlike other electromechanical models of an IPMC, the distributed nature of our model permits modelling the non-uniform bending of the material. Instead of modeling the tip deflection or uniform deformation of the material, we model the changing curvature. The transient behavior of the electrical signals as well as the transient bending of IPMC are described by Partial Differential Equations. Implementing the proper initial and boundary conditions results with the analytical description of the possibly nonuniform transient behavior of IPMC.

Keywords: IPMC, Lossy distributed RC lines

1. INTRODUCTION

IPMCs are materials that bend in electric field (Figure 1). An IPMC actuator consists of a highly swollen polymer sheet, such as NafionTM, filled with water or ionic liquid and plated with metal on both sides. Applied voltage causes the migration of ions inside the polymer matrix which in turn causes the non-uniform distribution of the ions inside the polymer. As a result, the polymer sheet bends. The direction of bending depends on the polarity of the applied voltage. An overview of the working principle of actuators can be found e.g. IPMC in (Shahinpoor, 2003).

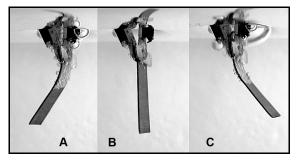


Figure 1. An IMPC sheet in a bent configuration with the opposite driving voltage polarities (A and C) and an initial configuration with no electric stimulus applied (B).

IPMC actuators and sensors have many appealing properties from the implementation point of view. Being noiseless, soft and flexible, mechanically simple, lightweight and resilient they have potentially many applications in the areas of noise damping, haptics, smart textiles, biorobotics, medicine, space applications and elsewhere (Shahinpoor and Kim, 2005). The state-of-the-art of the IPMC sensor and actuator technology is not thoroughly understood which makes it difficult to predict the behavior of this material and therefore limits the potential applications areas.

Several models are proposed so far to model the behavior of IPMC sensors and actuators. A systemized overview of the existing models can be found in (Kothera, 2005). The most accurate IPMC models are derived from first principles and comprise the modeling of underlying electrochemical phenomena coupled to the mechanical bending of the sheet (Nemat-Nasser and Thomas, 2004; Asaka and Oguro, 2000; Tadokoro et al., 2004). While capturing the complex phenomena inside the IPMC actuator those models tend to be complex. computationally time consuming and require laborious parameter identification.

The empirical models describing the behavior of the actuator on a macro-level are derived experimentally by curve fitting (Mallavarapu and Leo, 2001; Kanno et al. 1995) or based on the description of some sort of an equivalent circuit (Kanno et al. 1996; Bonomo et al. 2007; Newbury and Leo 2003). Kanno et al. (1996) have proposed a model in a form of an RC-line but by representing the circuit in a form of a first order transfer function they reduce it to a lumped model and define the relationship between tensile stress and input current. Also the model proposed by Bao et al. (2002) is based on the assumption of uniform properties but it is recognized that the distributed model would provide a more accurate description. Yim et al. (2006) propose a distributed model, where the IPMC actuator is divided to segments, but each segment is assumed to be driven separately to achieve waving motion of the actuator and each segment is again treated as a lumped model subjected to uniform tensile forces.

The models proposed so far can model the tip displacement or output force of the tip but not the configuration of the entire actuator surface. The model proposed by us is different in the sense that it takes into consideration the fact that deformation of the IPMC material is nonuniform. Figures 1 and 2 represent a typical behavior of the actuator where the bending curvature from the electric contacts along the sheet decreases.

The fact that the electric current through the polymer matrix of IPMC causes nonuniform distribution of voltage along the electrodes seems not to have been sufficiently covered in scientific literature. In this paper we propose modelling the IPMC actuator as a distributed RC line. This presentation permits identifing the electric current through the polymer matrix at every point of the IPMC sheet. As such, it corresponds more accurately to the real situation where the bending curvature of the actuator at each point is determined by the migration of ions at that particular location and variations in the ion concentration cause non-uniform bending.

We represent the model of an IPMC actuator in an analytical or simulated form based on the theory of RC transmission lines and show the solution in case of the step input voltage. By coupling the current through the polymer matrix to the mechanical bending of the actuator we derive the electromechanical model of an IPMC. We then proceed by representing the simulation results and thereafter demonstrate that these results are well consistent with the experimental data obtained from the experiments of four different types of IPMC.

2. CHARACTERIZATION OF THE ACTUATOR.

Generally the models of an IPMC described in the scientific literature do not characterize the shape of IPMC-based devices. These models usually describe the motion of the tip or the bending radius of the device assuming that the bending radius is constant. The equipment used to characterize the parameters such as for instance laser position sensors or force gauges (Jung et al. 2003, Richardson et al. 2003, Bandopadhya et al. 2006).

In order to describe the mechanical motion of the actuator, we developed a simple computer vision system. It consists of a fast CCD camera and a PC with image processing software. The National Instruments Vision was used for both frame grabbing and image processing. The direction of the camera is set transverse to the actuator and the experiment is illuminated from the background through a frosted glass. In perfect conditions the image of the actuator recorded in such a way consists of a single contrast curved line. It is easy to use image processing software to process the shape of the actuator during each particular frame. The separate frames of a noticeably bending actuator, recorded in such a way, are depicted in Figure 2.

It is apparent from Figure 2., that in the beginning of the input pulse (images 0...0.4s in Figure 2.-A) the actuator performs a sharp motion close to the input contacts only, the free end remains almost straight.

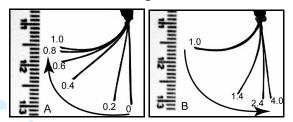


Figure 2. Overlay of a series of frames showing the response of an actuator to a 1s driving voltage pulse. A – actuation during the pulse; B – relaxation after the pulse. The numeric characters indicate the time instant of the frame.

Later (images 0.4...1.0s in Figure 2.-A) the flexure of the actuator propagates gradually on, but the flexure at the region close to the contacts does not increase any more. During the relaxation (images 1.0...4.0s in Figure 2.-B) the sharp decrease of the flexure takes place close to the input contacts again, whereas the remaining part of the actuator straightens slowly in few seconds.

The drop of voltages along the electrodes of the actuator can be recorded by attaching additional terminals onto its surface. The outline of the setup of the electrical measurements is depicted in Figure 3.

We measure the voltages on the surface of a working IPMC-based actuator or sensor by attaching a set of pairs of lightweight contacts to its surface using special lightweight clips, and connect them via thin wires to the measuring equipment. Voltages U_C , U_D , U_E and U_F with respect to the ground are measured at the

contacts C, D, E and F respectively, as well as the input voltage U_A at the contact A. The voltages between the two faces of the sample can be calculated as $U_C - U_D$, and $U_E - U_F$.

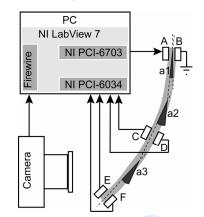


Figure 3. Setup of electrical measurements.

The measured voltages on an actuator, bending similarly to the one presented in Figure 2, are represented as a 3D graph in Figure 4.

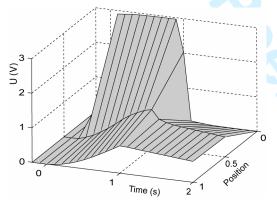


Figure 4. Voltages along a bending actuator.

It is apparent from Figure 4. that even in the middle of the sample the voltage does not reach a substantial value. The voltage at the free end only slightly differs from the voltage in the middle.

In order to describe the bending movement of the actuator, the image of the bending sheet is divided into segments assumed to have a constant curvature. The principle of determining the angles is shown in Figure 3. (angles a1 - a3). The angles of the segments are calculated from each frame of the video. The changing flexure of the actuator, electrically characterized in Figure 4. is depicted in Figure 5. It can be observed that the bending of the sheet is faster and stronger close to the input contacts, getting progressively weaker as well as delayed towards the free end of the sheet.

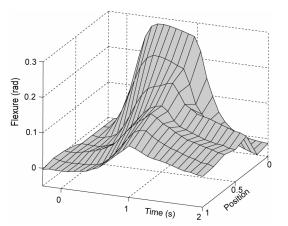


Figure 5. Mechanical response of an actuator to a step input voltage. The "Position" axis stands for the relative coordinate starting from the input contacts.

It is apparent that the two graphs – the graph of spreading voltages along the surface and the graph of bending angles along the surface are strikingly similar.

3. A DISTRIBUTED MODEL OF IPMC.

The fact that the electrical perturbation as well as the change of the flexure spreading along the actuator at finite speed; and the described similarity between the two graphs Figure 4. and Figure 5. were the motivations to develop a distributed model of an IPMC.

The basis of the model is the distributed model of an IPMC proposed by Kanno et al. (1996). Originally Kanno divided a piece of an IPMC into ten similar segments and modelled the relation between the input current and tip displacement. Dividing the same piece into an infinite number of infinitesimally short similar segments, gives an RC transmission line. The resulting distributed RC line represented by a series of equivalent circuits with discrete elements is depicted in Figure 6. The transient behavior of electrical signals, for instance voltage, electric current, charge, etc. along this kind of lines can be described with Partial Differential Equations (PDE) implementing the proper initial and boundary conditions.

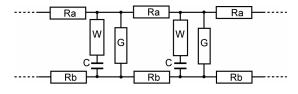
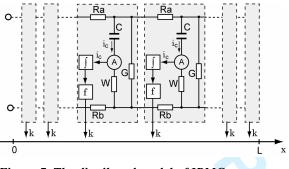
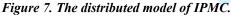


Figure 6. The distributed RC line describing IPMC, represented by a series equivalent circuits with discrete elements.

The distributed model of IPMC represented by an infinite series equivalent circuits with discrete elements of infinitesimally short single units is given in Figure 7. The conductivity of the electrodes of IPMC is represented by the series of resistances of the opposite electrodes Ra and Rb, connecting the single units. Each single unit contains the electrical parameters determining the propagation of voltage along the transmission line and the elements for calculating the mechanical behavior of the actuator within the limits of that unit.





There are two fundamental causes of the electric current between the electrodes of an IPMC through the polymer matrix:

- 1. The current caused by ionic conductivity. Relocating ions constitute the pseudocapacitance of the double-layer which forms at the interface between the ion exchange membrane and the metal electrode (Sadeghipour et al. 1992). As described hereinabove, the resulting irregular density of hydratized ions is the cause of bending of the IPMC. The resulting deformation of the IPMC is proportional to the total amount of relocated ions. In the equivalent circuit the pseudocapacitance is depicted as shunt capacitors C between the electrodes in each single unit. The conductivity W denotes the summarized transversal ionic conductivity of the electrodes and the ionomer.
- The current caused by electrochemical 2. electrode reactions, for example electrolysis of the solvent. The electrode reactions appear only if the voltage between the electrodes exceeds some certain critical level. depending on the materials used. The presence of the electrode reactions wastes energy and affects the propagation of voltage, but does not have direct effect on the deformation of the IPMC. In the equivalent circuit the electrode reactions are

depicted as shunt resistors G between the electrodes in each single unit.

The electric charge qdetermines the mechanical flexure k within the limits of the single unit. As the electric charge can be expressed as the derivative of the current with respect of time, the total electric charge qcarried over within each single unit is calculated as an integral of current i_C . Figuratively, each single unit of the RC distributed line contains a block composed of ammeter, measuring current i_C through the capacitance C, an integrator in order to determine the charge moved over within the limits of that unit, and function f describing the bending effect of a charge, moving to the electrode. In the simplest case the flexure is proportional to the charge and the block fcontains

$$k = \Upsilon q , \qquad (1)$$

where Υ is is the coefficient for the bending effect of the charge.

4. THE ANALYTICAL EQUATIONS DESCRIBING THE DISTRIBUTED MODEL OF IPMC

When the input current is switched to the one end of a circuit depicted in Figures 6 or 7, the current flows through all chains C - W and G. According to Ohm's Law, the current induces voltage drops on the resistances Ra and Rband the voltage across the line diminishes until the equilibrium state reaches. In the course of charging of the capacitive elements C the voltages and currents change, but at every time instant the system remains in its equilibrium state. This transient behavior can be described by PDE-s.

The step response of a system is the output of the system when a unit step function is used as the input and it is a common analysis tool used to determine certain metrics about a system. As we show hereinafter, the step response of the distributed line depicted in Figure 6. is solvable in an analytical form. On the other hand it is easy to verify the theoretical model by applying the step voltage to the input of the IPMC actuators, describing their electromechanical response and measuring the transient behavior of the electrical parameters.

In this section we give the equations describing the transient behavior of the voltage

u(x,t) for the distributed line of the finite length L depicted in Figure 6. when a voltage step is applied to its input. The derivation of the PDE and the procedure of applying the initial and boundary conditions is described in detail in (Punning and Jalviste, 2008) and is based on the solution of the heat equation with different boundary conditions (Powers, 2006; Kreyszig, 2006). We give only the short overview and the relevant equations in the current paper. From the analytical solution describing the transient behavior of voltage we derive the transient behavior of the charge q(x,t) of the capacitive element C, actually determining the amount of bending of IPMC, for example in the simplest case following the equation (1).

First, we transfer the line depicted in Figure 6. into the *Cauer canonical form* (Szekely, 2003) by replacing the two resistances Ra and Rb by their sum R = Ra + Rb. The resulting line is depicted in Figure 8.

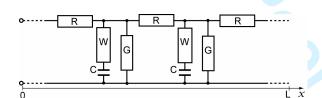


Figure 8. The Cauer canonical form of the line depicted in Fig. 6.

As shown in Figure 9, the parameters R and C are the resistance of the conductive layer and the capacitance of the dielectric per unit length of the line, respectively. The loss parameters Wand G are the transversal conductivities per unit length along the line. For visual clarity in Figure 9 the parameters R, C, G, and W, all defined per unit length along the coordinate x, are represented as discrete elements of a single cell of the line. The voltage checkpoints and the selected positive directions of the currents are indicated by arrows. We assume that all these parameters are uniform and time-invariant. Voltages and currents are assumed to be functions of the coordinate along the line and time, i.e. $i \equiv i(x,t)$, $i_C \equiv i_C(x,t)$, $i_G \equiv i_G(x,t)$, $u \equiv u(x,t)$, and $u_C \equiv u_C(x,t)$.

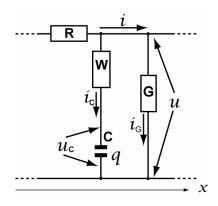


Figure 9. The meaning of the line parameters, voltages and currents for the distributed line.

In the next sections we give the equations describing the behavior of voltage, charge, water carried over and bending radius.

4.1. Behavior of voltage

The variation of current along the coordinate x at instant t is equal to the sum current through the chains "C - W" and "G":

$$\frac{\partial}{\partial x}i(x,t) = -(i_c(x,t) + i_G(x,t)), \qquad (2)$$

$$i_{G}(x,t) = Gu(x,t) .$$
(3)

The variation of voltage along the coordinate x is equal to the voltage drop on resistance R:

$$\frac{\partial}{\partial x}u(x,t) = -Ri(x,t) . \tag{4}$$

Current $i_C(x,t)$ charging the capacitance C is given by

$$i_{C}(x,t) = C \frac{\partial}{\partial t} u_{C}(x,t) .$$
⁽⁵⁾

Voltages in the chain C - W add up to the line voltage:

$$u(x,t) = u_C(x,t) + \frac{1}{W}i_C(x,t) .$$
(6)

Now we have 4 equations with 4 unknown variables: i(x,t), $i_C(x,t)$, $u_C(x,t)$ and

u(x,t). After some substitutions and rearrangements we get the PDE describing the transient behavior of voltage u(x,t) along the line in the form

$$\frac{\partial^{3}}{\partial x^{2} \partial t} u(x,t) + \frac{W}{C} \frac{\partial^{2}}{\partial x^{2}} u(x,t) - R(W+G) \frac{\partial}{\partial t} u(x,t) - \frac{RGW}{C} u(x,t) = 0.$$
(7)

This equation can be easily solved by a method called the separation of variables. The general solution of the PDE (7) for u(x,t) is

$$\cos(\omega x))e^{-\frac{W(\omega^2+RG)}{C(\omega^2+RG+RW)}t}, \quad (8)$$

 $u(x,t) = (A\sin(\omega x) + B\cos(\omega x))e^{-C(\omega^{-}+RG+RW)}$, (8) where *A* and *B* are arbitrary constants, with values determined from the boundary conditions.

Next, we introduce the term *"steady voltage* distribution". After a long time $(t \rightarrow \infty)$ under a constant input voltage the capacitance C finally charges completely and the voltages u(x,t) and $u_C(x,t)$ are equalized, $u(x) = u_C(x)$. As it can be inferred form Figures 8 9, the steady current through the distributed resistive network, formed by R and G, still remains. This results in a diminishing steady voltage, denoted by $u_{ST}(x)$, along the line. The equation describing the steady voltage distribution is $\frac{\partial^2}{\partial x^2} u_{ST}(x) = RGu_{ST}(x)$. (9)

By applying the condition of the input voltage U at x = 0: $u_{ST}(0) = U$, and the open end condition, $i_{ST}(L) = 0$ or

 $\frac{\partial}{\partial x}u_{ST}(L) = 0$, to its general solution

$$u_{ST}(x) = Ae^{\sqrt{RGx}} + Be^{-\sqrt{RGx}}$$
, we find that

$$u_{ST}(x) = U \frac{\cosh(\sqrt{RG(x-L)})}{\cosh(\sqrt{RGL})}.$$
 (10)

It is self-evident that when the input of the initially charged line is shorted, the capacitance C finally discharges through the resistive network and the shorted input, and the steady voltage is zero: $u_{ST}(x) = 0$.

The initial/boundary conditions can be applied to the equation (8) using the method of Fourier series. This procedure is thoroughly described in (Punning and Jalviste, 2008). Naturally, it is possible to define many different initial/boundary conditions to (8), that result in an analytical solution. In the current paper we describe only the two distinct cases of practical importance:

 A) the step voltage of amplitude normalized to 1 is applied to the input of the initially discharged line. The initial and boundary conditions for this case are:

a. initial voltage distribution: u(x,0)=0

- b. input voltage at x=0: u(0,t) = 1
- c. open end condition: $\frac{\partial}{\partial r}u(L,t)=0$
- d. steady voltage distribution:

$$u_{ST}(x) = \frac{\cosh(\sqrt{RG}(x-L))}{\cosh(\sqrt{RG}L)}$$

B) the shorted input to the line that has been under the input of voltage of amplitude of 1 until the steady distribution is formed. The initial and boundary conditions for this case are:

a. initial voltage distribution:

$$u(x,0) = \frac{\cosh(\sqrt{RG(x-L)})}{\cosh(\sqrt{RGL})}$$

b. input voltage at x=0: u(0,t) = 0

- c. open end condition: $\frac{\partial}{\partial x}u(L,t)=0$
- d. steady voltage distribution: $u_{ST}(x)=0$

In general, the voltage-step response of the distributed lines of length L depicted in Figure 8. can be expressed as

$$u(x,t) = U \sum_{n=1}^{\infty} (b_n \varphi(\omega_n x) e^{-k_n t}) + u_{ST}(x), \quad (11)$$

where

$$k_n = \frac{W(\omega_n^2 + RG)}{C(\omega_n^2 + RG + RW)},$$
(12)

and where $\varphi(\omega_n, x)$, ω_n , b_n , and $u_{ST}(x)$ are the eigenfunctions, eigenvalues, Fourier coefficients, and the steady voltage distribution respectively. All these quantities depend on the initial/boundary conditions. Applying the boundary conditions for our two cases, we get that the solutions for voltage are:

A)
$$u(x,t) = \sum_{n=1}^{\infty} \left(-b_n \sin\left(\frac{2n-1}{2L}\pi x\right) e^{-k_n t} \right) + \frac{\cosh(\sqrt{RG}(x-L))}{\cosh(\sqrt{RG}L)}$$
(13)

B)
$$u(x,t) = \sum_{n=1}^{\infty} \left(b_n \sin\left(\frac{2n-1}{2L}\pi x\right) e^{-k_n t} \right)$$
 (14)

where

$$k_n = \frac{W(4RGL^2 + \pi^2(2n-1)^2)}{C(\pi^2(2n-1)^2 + 4RL^2(G+W))}$$
(15)

and

$$b_n = \frac{4\pi (2n-1)}{\pi^2 (2n-1)^2 + 4RGL^2}.$$
 (16)

4

5

6

7

8

9

10

11

12

13

14

15

16

17 18

19

20

21

22 23

24

25

27

28

29

30 31

32

35

40

41

42

43

44

45

46

47

48

49

50

51

52

53

54

55

56

57

58

59

60

4.2. Behavior of charge

As described hereinabove, the mechanical flexure of the actuator k(x,t) is determined by the transitory charge q(x,t) of the capacitance C. The PDE describing the behavior of the charge can be derived similar to the derivation of the PDE for voltage in the previous chapter. Using the relation describing that the current through the capacitor is the derivative of its charge by time

$$i_{C}(x,t) = \frac{\partial}{\partial t}q(x,t)$$
(17)

and the relation between the charge and voltage of a capacitor

$$u_C(x,t) = \frac{1}{C}q(x,t), \qquad (18)$$

it is possible to convert the equations (2)-(6) to 4 new equations with 4 unknown variables: i(x,t), $i_C(x,t)$, q(x,t) and u(x,t). From

these equations it is easy to derive the PDE describing the behavior of the charge q(x,t):

$$\frac{\partial^3}{\partial x^2 \partial t} q(x,t) + \frac{W}{C} \frac{\partial^2}{\partial x^2} q(x,t) - R(W+G) \frac{\partial}{\partial t} q(x,t) - \frac{RGW}{C} q(x,t) = 0.$$
(19)

It is intriquing that the PDE-s describing the behavior of voltage (7) and the charge (19) are exactly similar. The difference between the two stands only in the initial and boundary conditions. The general solution for the charge q(x,t) is similar to (8):

$$q(x,t) = (A\sin(\omega x) + B\cos(\omega x))e^{-\frac{W(\omega^2 + RG)}{C(\omega^2 + RG + RW)}t}.$$
 (20)

Nevertheless it is not possible to apply the initial/boundary conditions to (20) using the method of separation of the variables, because the charge q(0) at the boundary x = 0 is not constant but some unknown time-dependent function.

Instead, we derive the behavior of the charge q(x,t) from the equation (6). Using the relations (17) and (18) we can write

$$u(x,t) = \frac{1}{C}q(x,t) + \frac{1}{W}\frac{\partial}{\partial t}q(x,t).$$
(21)

Solving (21) for q(x,t) gives

$$q(x,t) = \left(\int_{0}^{t} Wu(x,\tau) e^{\frac{W}{C}\tau} d\tau + \rho(x)\right) e^{-\frac{W}{C}t}, \quad (22)$$

where $\rho(x)$ is the constant of integration. From the boundary conditions we can find that $\rho(x)$ equals to the initial distribution of charge corresponding to the initial voltage distribution at t = 0. For the case A) the initial distribution of charge is self-evidently zero: $\rho(x) = 0$. For the case B) the initial charge $q_{ST}(x)$ can be found from the final steady voltage distribution of case A) as

$$\rho(x) = Cu_{ST}(x), \tag{23}$$

where $u_{ST}(x)$ is defined by (10).

After substituting the behavior of voltage described by (13) or (14) and the corresponding steady charge distribution into (22) we get the behavior of the charge q(x,t) along the line for our two cases.

4.3. Hydraulic pressure

The bending movement of IPMC is produced by the hydraulic pressure caused by the moving hydratized charge. In the simplest case the amount of water carried over by the migrating cations is proportional to the charge:

$$k(x,t) = \Upsilon q(x,t), \qquad (24)$$

where Υ is the coefficient of hydratization of the cations.

Several authors have described the slow back-relaxation of the IPMC actuators after the quick response to the applied voltage (Bao et al. 2002; Shahinpoor, 2003). This phenomenon is explained with the water leakage resulting from a high-pressure layer near the cathode toward to the anode through channels in the polymer backbone. The research of the effect of relaxation and developing the equation for the hydraulic pressure considering the backrelaxation, suitable for the distributed model of IPMC is the subject of our future work.

4.4. Bending radius

The derivation of the relation between the curvature of the swollen polymer matrix and the charge carried over is described in Berry and Pritchet, 1984). The equations are derived similar to those employed by Timoshenko in his work on bi-metallic strips (Timoshenko, 1925). Actually Berry and Pritchet describe the method of determining the coefficient of moisture swelling of polymers by their bending curvature. In our model of IPMC we use the result conversely - determine the bending curvature

from the nonuniform concentration profile of liquid inside the polymer

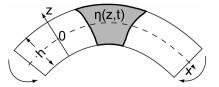


Figure 10. Self-induced bending of a polymer strip caused by the water concentration profile $\eta(z,t)$ through the polymer layer.

Assuming that the polymer is isotropic and swells in volume V proportionally to a uniform water concentration η_0 , we may write

$$\varepsilon = K\eta_0, \tag{25}$$

where ε is a hygroscopic strain analogous to a thermal expansion strain of the bi-metal thermostats, and K is a linear swelling parameter equal to one-third of the volumetric swelling factor:

$$K = \eta_0 \frac{1}{3} \frac{\Delta V}{V} \tag{26}$$

A nonuniform concentration profile of water $\eta(z,t)$ through the thickness (z-coordinate) of the strip will produce elongation, bending and internal stress. With the assumption that plane cross-sections remain plane, the stress $\sigma(z,t)$ is given by

$$\frac{\sigma(z,t)}{E_1} = K\eta(z,t) - \varepsilon_0(t) - \frac{z}{r(t)},$$
(27)

where E_1 denotes $\frac{E}{(1-\nu)}$, E and ν are

Young's modulus and Poisson ratio of the polymer layer, $\varepsilon_0(t)$ is the strain at midplane

z = 0, and r(t) is the radius of curvature. Since the polymer layer is under no external forces, we can write

$$\frac{1}{r(t)} = \frac{12K}{h} \int_{-1/2}^{1/2} \eta(s,t) ds$$
(28)

where we introduced the dimensionless coordinate $s = \frac{z}{h}$ for convinience.

Assuming that concentration profile of water through the thickness (z-coordinate) of the strip is linear: $\eta(x, s, t) = s \mu(x, t)$, the equation (28) reduces to

$$r(x,t) = \frac{h}{K\mu(x,t)}$$
(29)

4.5. Behavior of electric current

The distribution of electric current between the opposite electrodes cannot be measured directly on an IPMC sample. Nevertheless it can be derived from the previous equations. As described in Chapter 3, by means of the bending movement of IPMC it can be divided into two parts. The current caused by ionic conductivity $i_C(x,t)$, described by (17), is related to the behavior of charge q(x,t), actually producing movement. The current caused by the electrochemical electrode reactions $i_G(x,t)$, described by (3) it is an useless waste of energy with regard to producing the bending motion Both currents participate in determining of the distribution of voltage and the charge and hence, the bending movement of the actuator.

The total input current $i_{in}(t)$ of the sample is determined by all currents over the full length of the distributed line:

$$i_{in}(t) = \int_{0}^{L} \left(i_C(x,t) + i_G(x,t) \right) dx$$
(30)

5. ESTIMATION OF THE PARAMETERS.

The values of the resistances of the surface electrodes of IPMC can be measured using a four-probe system. This method eliminates inexactnesses caused by the inconsistent current density and the resistances of the contacts.

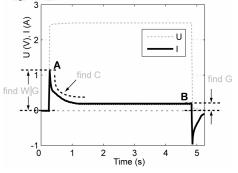


Figure 11. Response of the electric current to a rectangular voltage pulse.

The values of the parameters G, Q and C can be determined using a technique with voltage step pulses as follows. A small piece of the IPMC material is wholly fixed between contact clamps made of gold. In this configuration the resistance of the electrodes does not influence the results. The typical response of electric current corresponding to a long-lasting step voltage input is depicted in

60

Figure 11. Electric current peaks sharply at the very first moment (instant A). After charging the whole pseudocapacitor, electric current remains at a stable level (instant B).

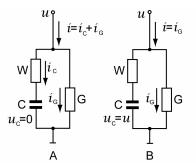


Figure 12. Estimation of the resistances G and W.

This behaviour of current can be explained by analysing the equivalent circuit illustrated in Fig. 12. At the very first moment, when the capacitor C is totally discharged, the current flows through the parallel resistances G and W(instant A). When the capacitance C is totally charged, the current flows through resistance Gonly (instant B). The capacitance C can be found from the decay of the electric current.

6. VERIFICATION OF THE MODEL

In order to prove the validity of the distributed model of IPMC, we present the actual behavior of different IPMC actuators and the computational results of the simulations using the equations given hereinabove. First we compare the behavior of the two fundamentally different IPMC materials, then the actuators made of the same material, but having different dimensions.

6.1. Behavior of actuators with different electrical parameters

The experiments show that the electromechanical responses of the different types of IPMCs are different. Some materials bend faster, some slower; some have almost constant bending radius, some bend nonuniformly. In order to demonstrate the validity of the distributed model of IPMC in the case of different materials, we compare the results of the experiments carried out with two fundamentally different IPMC materials manufactured by ourselves and the simulations of the distributed model of the IPMC using the estimated parameters. We give the parameters of the samples of both materials measured using the methodology described in Chapter 5, and present

the graphs of voltage and bending movement as described in Chapter 2. Simultaneously we simulate the same graphs by the equations given in Chapter 4. using the measured parameters and compare the measured and simultaed behaviors of the samples.

The IPMCs represented in the current paper are: *Sample1* - an IPMC covered with platinum electrodes using the method of electroless deposition; and *Sample2* - an IPMC covered with gold electrodes using the direct assembly method.

The parameters of the samples, measured using the methodology described in Chapter 5, are given in the Table1.

The Sample1 is made of 0.25 mm thick Nafion membrane and covered with platinum electrodes using the method of electroless deposition. It is a water-containing IPMC, intended to work in a wet environment. The cations introduced to the ionomer were Li⁺. This material is thick, hence more stiff than the other material. The thicker material contains potentially more cations, thus it has relatively big pseudocapacitance. The resistance of the electrodes of this sample is rather high, but still good enough to ensure conductivity. The nonuniform behavior of this sample is considerable due to the high resistance of the electrodes. The value of the conductivity W (see Figure 7.) is relatively high. When the applied voltage is lower than the voltage required for the electrolysis of water, the value of G is very low - in the range of about $10^{-4} \frac{1}{\Omega \cdot cm}$. When the applied voltage is close to the voltage required for the electrolysis of water, the conductivity Ggains sharply up to about $10^{-1} \frac{1}{\Omega \cdot cm}$.

Due to the high conductivity W and the relatively high resistance of the electrodes Ra and Rb, the nonuniform behavior of the Sample1 expresses extra intensely.

The experimental results of the voltage measurements and the electromechanical response of the Sample1 are depicted in Figure 4. and Figure 5. respectively.

The simulations of the Sample1 are given in Figure 16. The graphs demonstrate that voltage increases rapidly close to the input contacts and more slowly further away from the input contacts (Fig. 16.-A).

It is not possible to measure directly the distribution of electric current through the sheet.

This data can be only derived from the simulations, using the equation (17). The distribution of current depicted in Figure 16.-B produces the bending motion of the sample depicted in Figure 16.-C. The graph exhibits that the actuator performs a sharp movement only close to the input contacts. The noticeably weaker change of the curvature of the free end appears after a short delay. The behavior of the voltage and the flexure are rather similar to the parameters obtained by the measurements of a real actuator and presented in Figures 4. and 5. respectively.

The Sample1 exhibits insistent backrelaxation. As seen from Figure 5, already in a half second after the beginning of the input pulse. As we have no model for relaxation yet, we give here only the graphs for our case A - the step voltage is applied to the input of initially discharged actuator.

The Sample2 is an ionic liquid containing IPMC made of 0.18 mm thick Nafion membrane. It is covered by a thin layer of RuO_2 powder and gold foil electrodes glued to the ionomer with the dilution of nation. This material is intended to work in air. The conductivity of the surface of the gold electrodes of that material is very high, however the poor conductivity of the RuO₂ layer between the gold foil and the ionomer creates high value of W. The large surface area of the RuO₂ powder supposedly creates large pseudocapacitance of the IPMC material. The ionic liquid used was EMITf and the cations introduced to the polymer were Li^+ .

Due to the pure conductivity of the RuO_2 layer between the gold electrode and the ionomer the ionic current inside the ionomer cannot grow fast. For that reason the voltage drop along the electrodes is imperceptible and the IPMC has nearly a constant bending radius as depicted in simulations in Figure 13. As electric current between the electrodes cannot grow, this IPMC is slow. It gains its maximal flexure in minutes.

Sample2 performs a slow bending movement with almost uniform bending radius over its full length. During the 8 sec input voltage pulse it almost reaches the steady state. During the pulse the voltage along the sample is near to the uniform distribution, so that the drop of voltage occurs on the conductivity W.

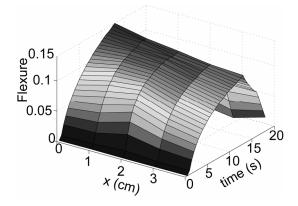


Figure 13. Measured mechanical response of Sample2.

The simulations of the charge, calculated according to (22) in the course of applied voltage and in the course of relaxation after the shorting of the input contacts are depicted in Figure 17.

The distribution of current between the opposite electrodes is depicted in Figure 17-B. While in the case of the nonuniform bending of Sample1 the current peaked only for a very short time near the contacts only as depicted in Figure 17-B, the current of Sample 2 is several magnitudes weaker, but remains almost uniform along its full length for a long time, producing uniform bending.

6.2. Behavior of actuators of different lengths

The length L of the IPMC actuators is one of the parameter of the model. According to the equations (22), (13) and (14) the transient behavior of the IPMC actuators is different in the case of the actuators having different length. The transient bending movement of a shorter actuator is not just similar to the first part of the longer one. In order to compare the transient bending behavior of the actuators of different lengths, we recorded some experiments of bending movement of a strip of IPMC, cut it shorter, and repeated the experiment. This method ensures that the electrical parameters of the strips are alike.

The driving signal of the actuator in the course of the experiments presented in the current paper is a rectangular pulse of the amplitude of 2V for all the experiments. The overlays of a series of frames are represented in Figure 18. It is clearly visible that the bending of the long actuator is inert and weak (Figure 18-A), while the bending of the the free tip of the almost twice shorter actuator (Figure 18-C) is much sharper and higher.

The photos of the strips of IPMC are depicted in Figure 14. The IPMC material used was MusclesheetTM provided by Biomimetics Inc in 2004. The parameters of the strips are given in Table1 as the *Sample3*

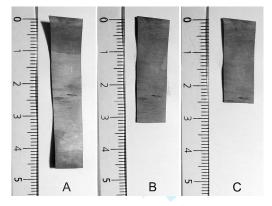


Figure 14. IPMC actuators of different lengths. A short slice is cut off from the same piece of IPMC in order to obtain the next one.

The simulated transient bending movements of the actuators of different lengths provided according to the equation (22) are depicted in Figure 15. The graphs exhibit that the amplitude of bending of the shorter actuator is higher and it is gained earlier than that of the longer actuators.

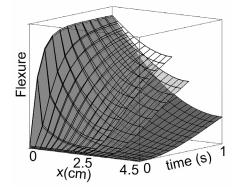


Figure 15. Simulated transient behavior of the IPMC actuators of different lengths made of the same IPMC material, drawn in the similar scale.

7. DISCUSSION

The presented distributed one-dimensional model of an IPMC consists of a number of lumped models coupling them with a spacial parameter - a generally uneven distribution of voltage caused by the resistance of the electrodes. It shows a good correlation with the experimental data obtained from the measurements conducted with the different

IPMC materials. Its advantages with respect to the previous models are:

- it permits modeling the non-uniform flexure of the IPMC actuator in spatial and time domain.
- it permits modeling large flexure of the actuator or sensor.
- it takes into account the real measurable parameters of the material – resistance of the electrodes and capacitance and with respect to the previously developed models does not reduce it to a uniform lumped model;
- it is scalable, i.e. the length of the actuator is one of the parameters of the model;
- the values of the measurable parameteres the capacitance of the material, the resistance of the electrodes and the length; may vary in a large scale.

The model described in the current paper gives the analytical solution for the free bending of the IPMC actuators only. It does not take into account the mechanical parameters of IPMC membranes, for example the viscoelasticity of polymer membranes, the blocking force produced by the IPMC actuator, inertia, etc. Presumably the combination of the electrical distributed model and the theory of mechanics of multilayer elastic thin films would give a result, capable to express the force produced by arbitrary segment of the actuator.

IPMC materials are also known to have sensor properties, When the material is mechanically deformed, it generates a weak voltage between the faces of the IPMC sheet due to the change of the concentration of ions. According to (2) voltage at output contacts depends on time and distance between the bending area and the output. If the deformation is continuous or distributed, the values of U(x,t)should be superpositioned. Verification of the proposed model for IPMC sensors is a subject of our future work.

8. ACKNOWLEDGEMENTS

This work has been supported by Estonian Ministry of Education, European Science Foundation, Estonian Science Foundation grants 6763 and 6765, and by Estonian Information Technology Foundation

Table1. The parameters of the samples

e1. The parameters of the samples										
	sample		thickness	Ra	Rb	W	G	С	cations	
		(mm)	of ionomer (µm)	$(\frac{\Omega}{cm})$	$(\frac{\Omega}{cm})$	$(\frac{1}{\Omega \cdot cm})$	$(\frac{1}{\Omega \cdot cm})$	$(\frac{F}{cm})$		
	1.	10 x 35	250	9	5	1	0.0005	0.02	Li ⁺	
	2.	10 x 35	180	0.5	0.5	0.015	0.0001	0.02	Li ⁺	
	3.	8 x XX	180	3	1.5	0.5	0.0015	0.05	Li ⁺	

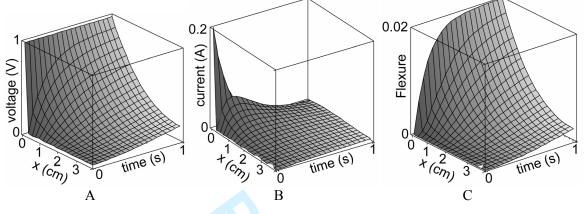


Figure 16. Simulations of Sample1. A – voltage, B – current, C – charge.

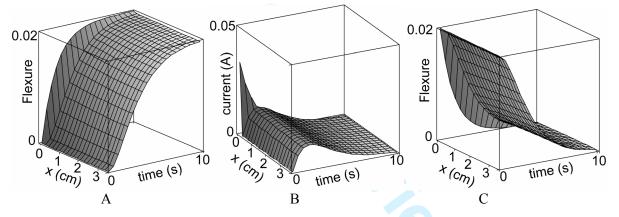


Fig. 17. Simulations of Sample2. A - charge during the step voltage input; B - current during voltage input; C - charge during relaxation.

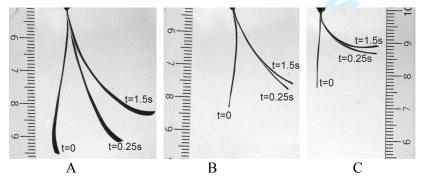
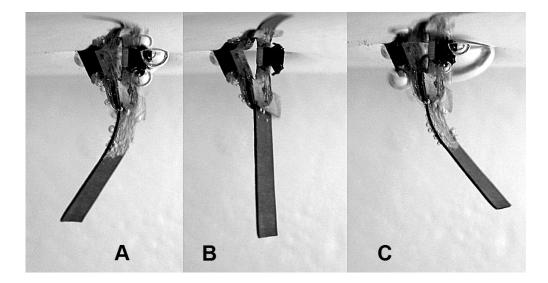


Fig. 18. Overlay of a series of frames of different time instants of 3 experiments with actuators made of the same material - Sample3. The time instants of the frames are the initial position (t=0s); in the middle of the bending (t=0.25s); and the steady position (t=1.5s).

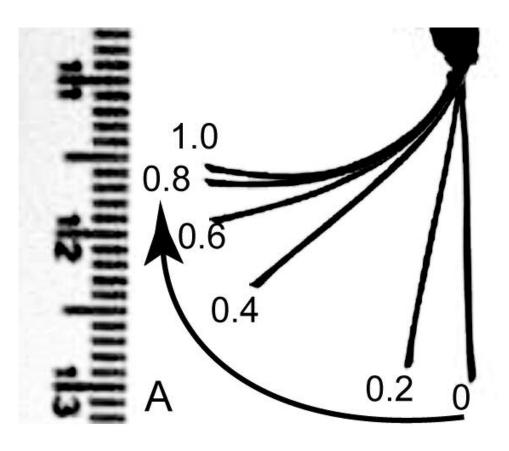
REFERENCES

- Asaka, K. and Oguro, K. 2000. "Bending of Polyelectrolyte Membrane-Platinum Composites by Electric Stimuli. Part II, Response Kinetics", J. Electroanal. Chem, 480:186-198
- Bandopadhya, D. et al. 2006. "Active vibration suppression of a flexible link using ionic polymer metal composite," Proc. IEEE Conference on Robotics, Automation and Mechatronics, 1-6.
- Bao, X. et al. 2002. "Measurements and Macro Models of Ionomeric Polymer-Metal Composites (IPMC)," EAPAD Conference 2002, Proc. SPIE (4695):286-293.
- Berry, B.S. and Pritchet, W.C. 1984 "Bending-cantilever method for the study of moisture swelling in polymers," IBM J. Res. Develop, 28(6):662-667
- Bonomo, C. et al. 2007. "A nonlinear model for ionic polymer metal composites as actuators", Smart Mater. Struct. 16:1-12.
- Jung, K. et al. 2003. "Investigations on actuation characteristics of IPMC artificial muscle actuator," Sensors and Actuators A: Physical, 107(2):183–192.
- Kanno, R. et al. 1995. "Modeling of ICPF Actuator, Modeling of Electrical Characteristics" Proc. IEEE 21st Intl Conf. On Industrial Electronics, Control, and Instrumentation, 2:913-918.
- Kanno, R. et al. 1996 "Linear approximate dynamic model of an ICPF actuator", Proc. IEEE Intern. Conf. on Robotics and Automation, 1:219-225.
- Kothera, C.S. 2005. "Characterization, Modeling, and Control of the Nonlinear Actuation Response of Ionic Polymer Transducers", Ph.D. dissertation, Dept. of Mechanical Engineering, Virginia Tech.
- Kreyszig, E. 2006. "Advanced Engineering Mathematics", 9th Ed., Wiley.
- Mallavarapu, K. and Leo, D. 2001. "Feedback Control of the bending response of ionic polymer actuators," Journal of Intelligent Material Systems and Structures, 12(3):143–155.
- Nemat-Nasser, S. and Thomas, C.W. 2004. "Ionomeric polymer-metal composites", in: Bar-Cohen, Y. (ed.), "Electroactive Polymer (EAP) Actuators as Artifical Muscles. Reality, Potential, and Challenges," SPIE Press, Washington.
- Newbury, K. and Leo, D. 2003. "Linear Electro-mechanical Model of Ionic Polymer Trans-ducers – Part I: Model Development", Journal of Intelligent Material Systems and Structures, 14(6):333–342.
- Punning, A. and Jalviste, E. 2008. "Analytical Solution for Voltage-Step Response of Lossy Distributed RC Lines", IEEE Transactions on Microwave Theory and Techniques. In print.
- Powers, D.L. 2006. "Boundary value Problems and Partial Differential Equations", Elsevier.
- Richardson, R.C. et al. 2003. "Control of ionic polymer metal composites," IEEE/ASME Transactions on Mecatronics, 8(2):245–253.
- Sadeghipour, K. et al. 1992. "Development of a novel electro-chemically active membrane and "smart" material based vibration sensor/damper," Smart Materials and Structures, 1:172–179.
- Shahinpoor, M. 2003. "Ionic polymer-conductor composites as biomimetic sensors, robotic actuators and artificial muscles – a review", Electrochimica Acta 48:2343-2353

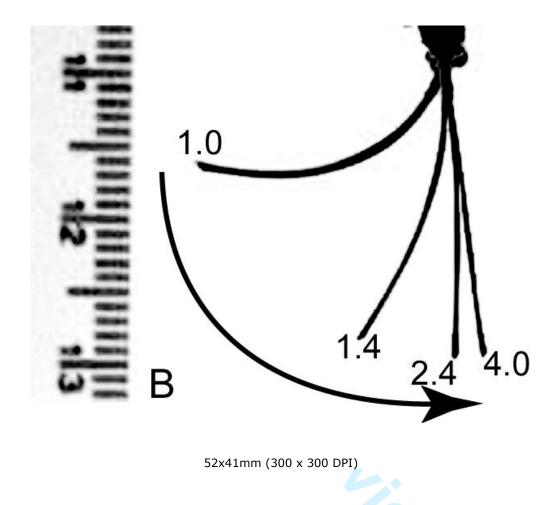
- Shahinpoor, M. and Kim, K.J. 2005. "Ionic polymer-metal composites: IV. Industrial and medical applications," Smart Materials and Structures, 14:197-214.
- Tadokoro, S. et al. 2004. "Modeling IPMC for Design of Actuation Mechanism" in: Bar-Cohen, Y. (ed.), "Electroactive Polymer (EAP) Actuators as Artifical Muscles. Reality, Potential, and Challenges," SPIE Press, Washington.
- Timoshenko, S.P. 1925. "Analysis of bi-metal thermostats," J. Opt. Soc. Am. 11:, 233-255.
- Yim, W. et al. 2006. "Dynamic Modeling of Segmented Ionic Polymer Metal Composite (IPMC) Actuator," Proc. IEEE/RSJ Int. Conf. on Intelligent Robots and Systems 5459-5464.



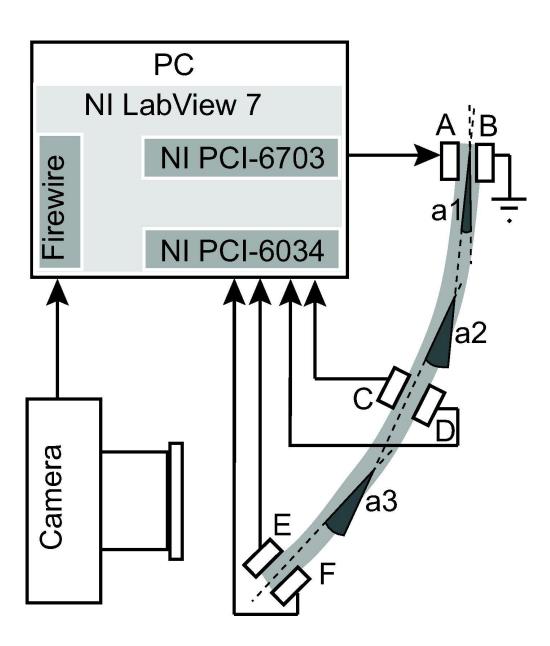
An IMPC sheet in a bent configuration with the opposite driving voltage polarities (A and C) and an initial configuration with no electric stimulus applied (B). 99x52mm (300 x 300 DPI)



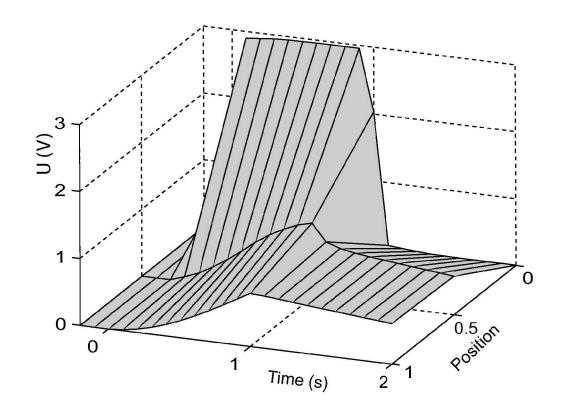
49x39mm (300 x 300 DPI)





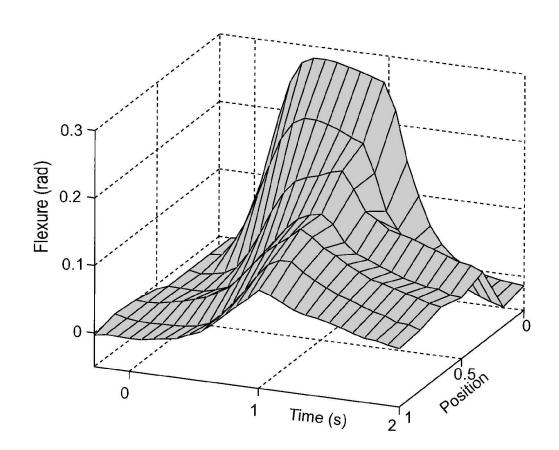


58x67mm (600 x 600 DPI)

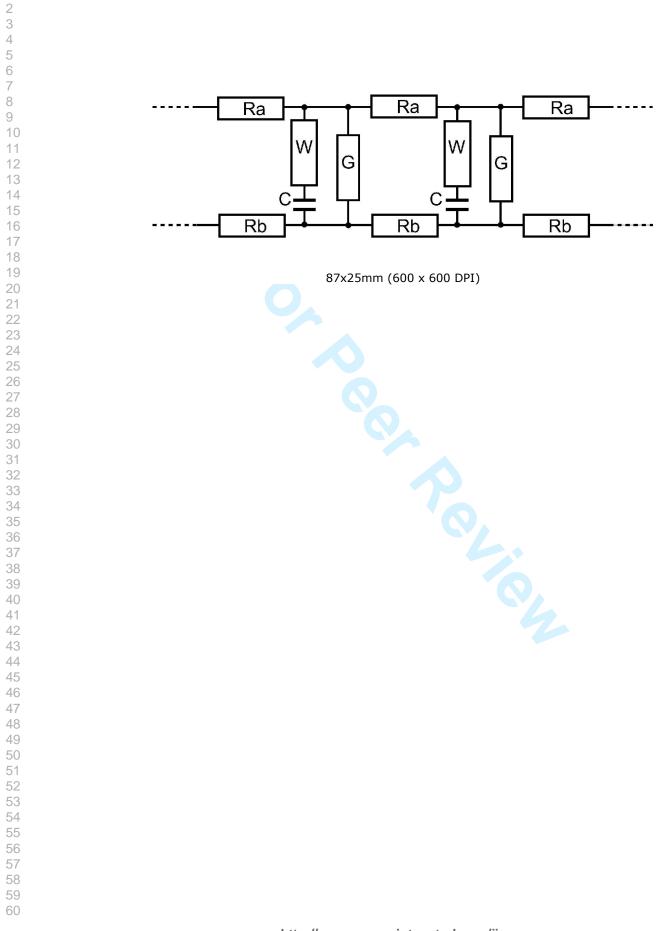


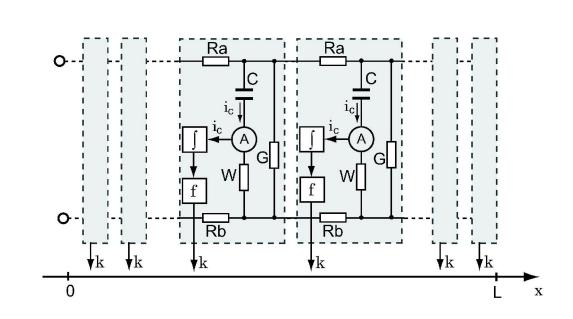
68x50mm (600 x 600 DPI)

Page 19 of 38



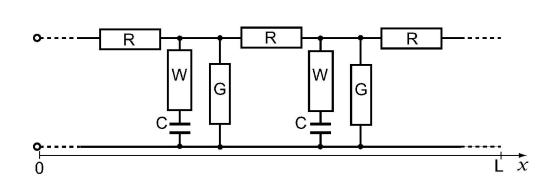
69x55mm (600 x 600 DPI)



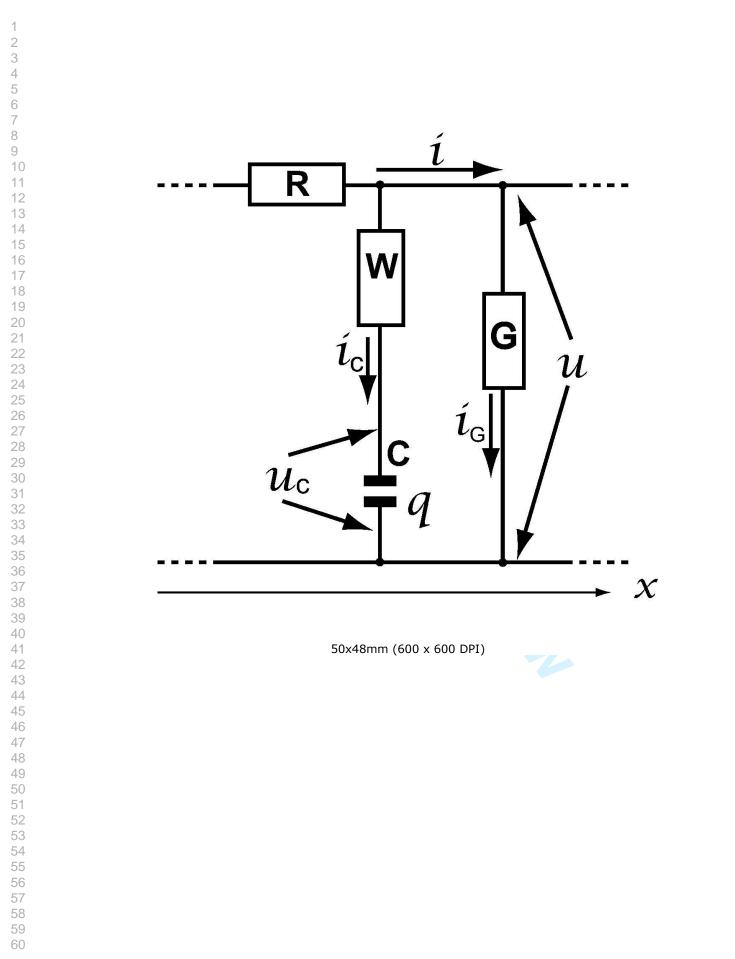


96x51mm (600 x 600 DPI)

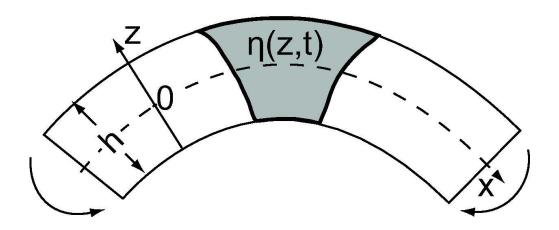




95x29mm (600 x 600 DPI)

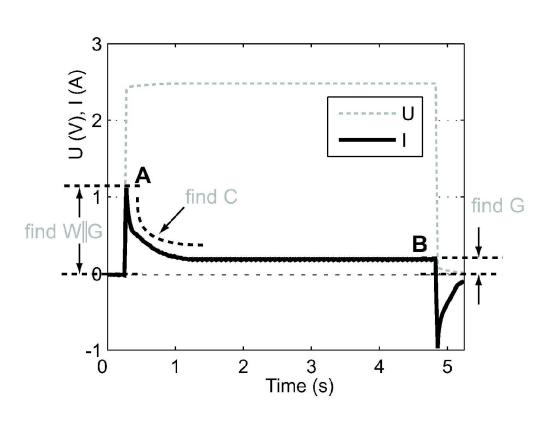




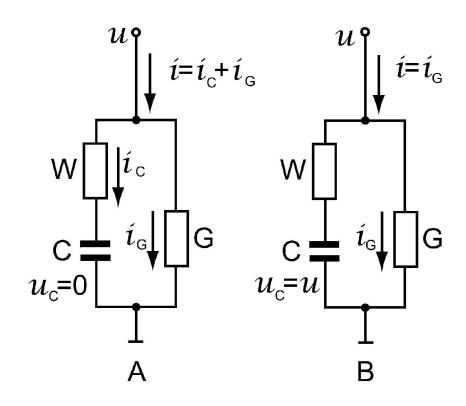


52x21mm (600 x 600 DPI)

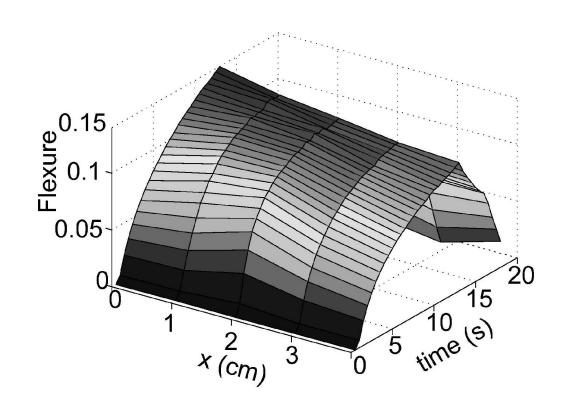




70x50mm (600 x 600 DPI)

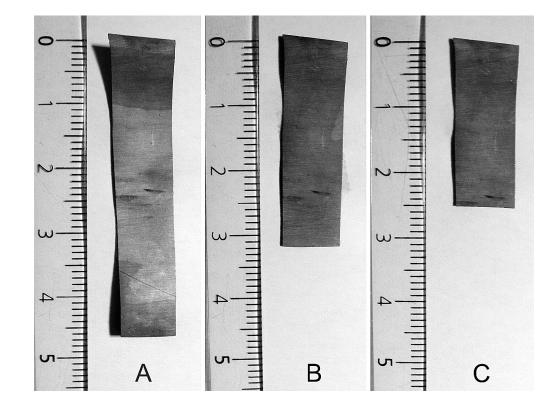


75x56mm (600 x 600 DPI)



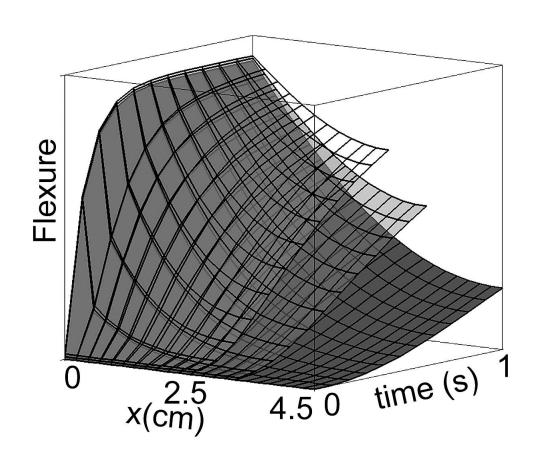
70x50mm (600 x 600 DPI)

http://mc.manuscriptcentral.com/jimss



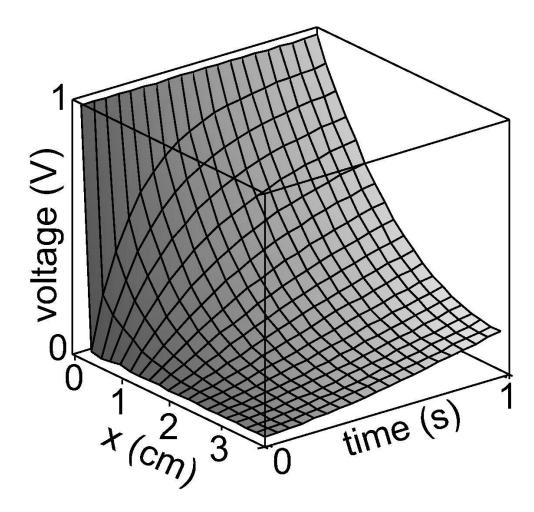
66x49mm (600 x 600 DPI)

Page 29 of 38



52x45mm (600 x 600 DPI)

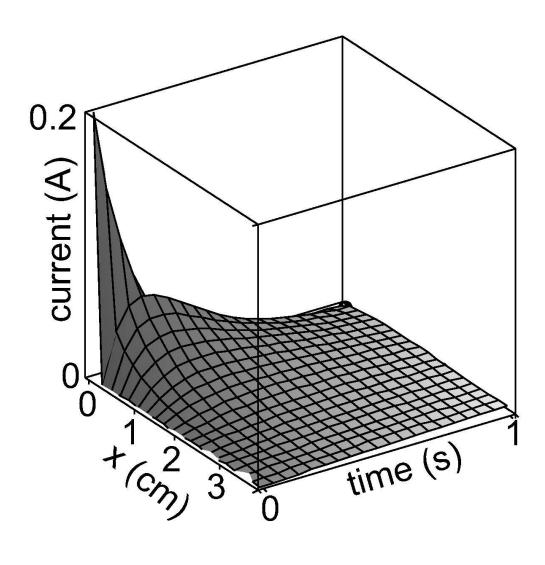
http://mc.manuscriptcentral.com/jimss



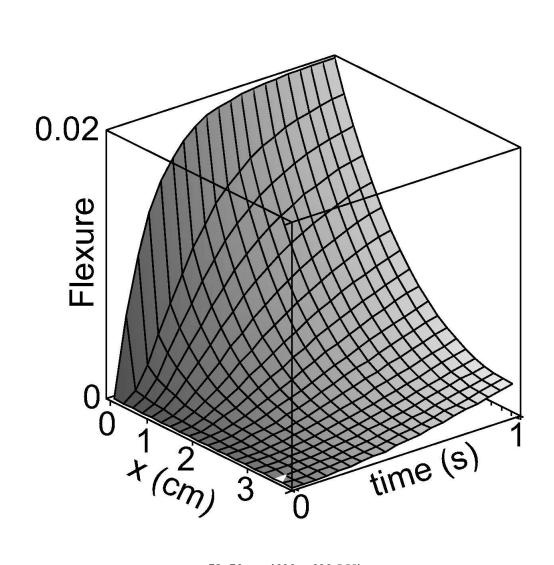
48x45mm (600 x 600 DPI)



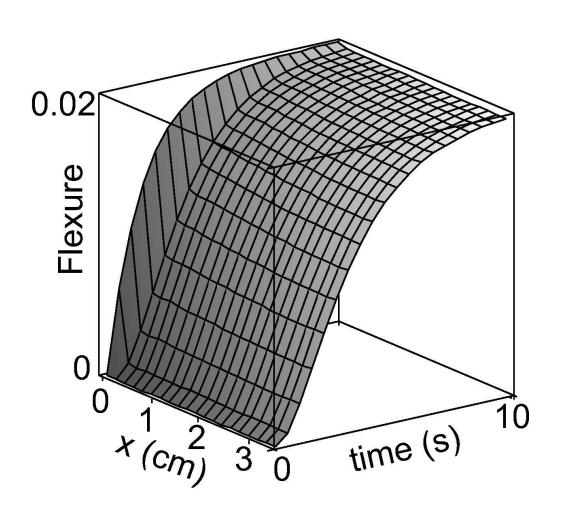
Page 31 of 38



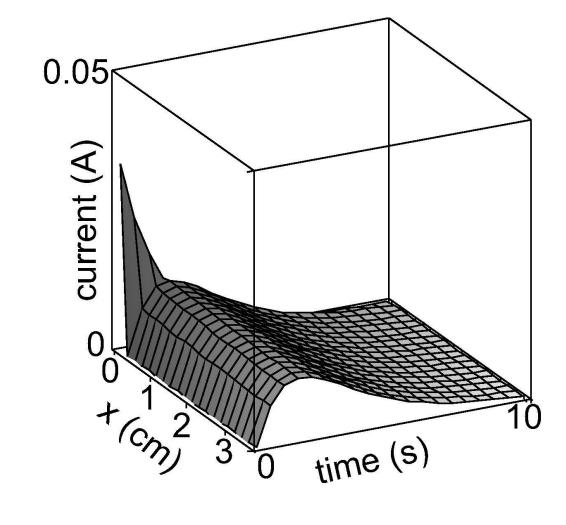
50x49mm (600 x 600 DPI)



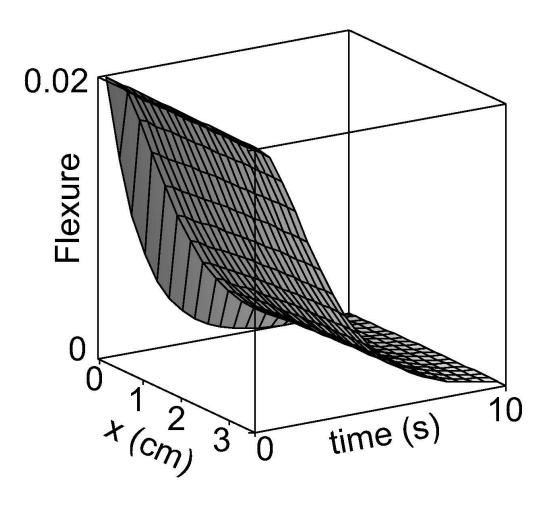
52x50mm (600 x 600 DPI)



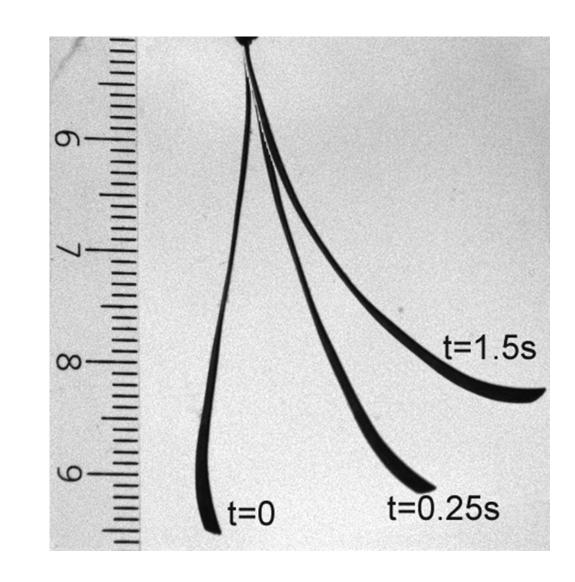
52x47mm (600 x 600 DPI)



51x48mm (600 x 600 DPI)

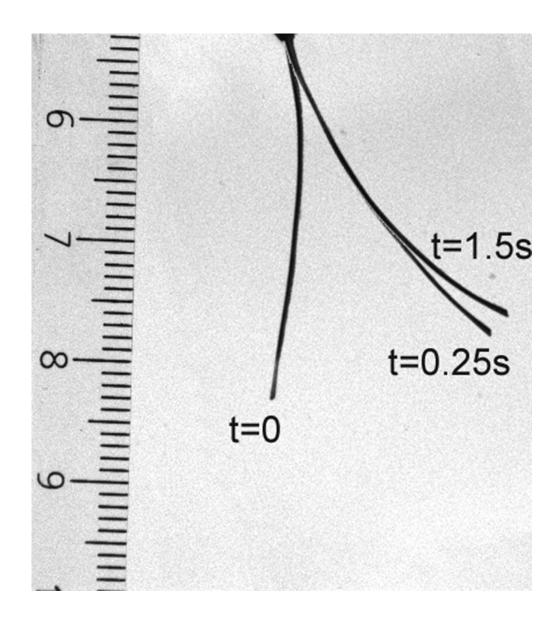


52x47mm (600 x 600 DPI)

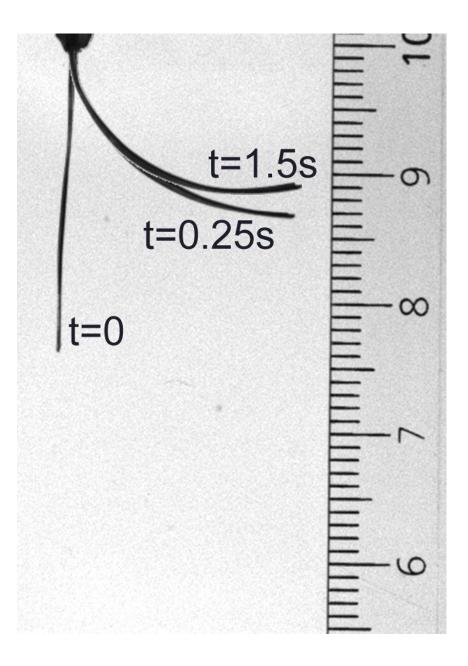


38x40mm (600 x 600 DPI)





35x40mm (600 x 600 DPI)



28x40mm (600 x 600 DPI)